

GTO-on-a-Chip System

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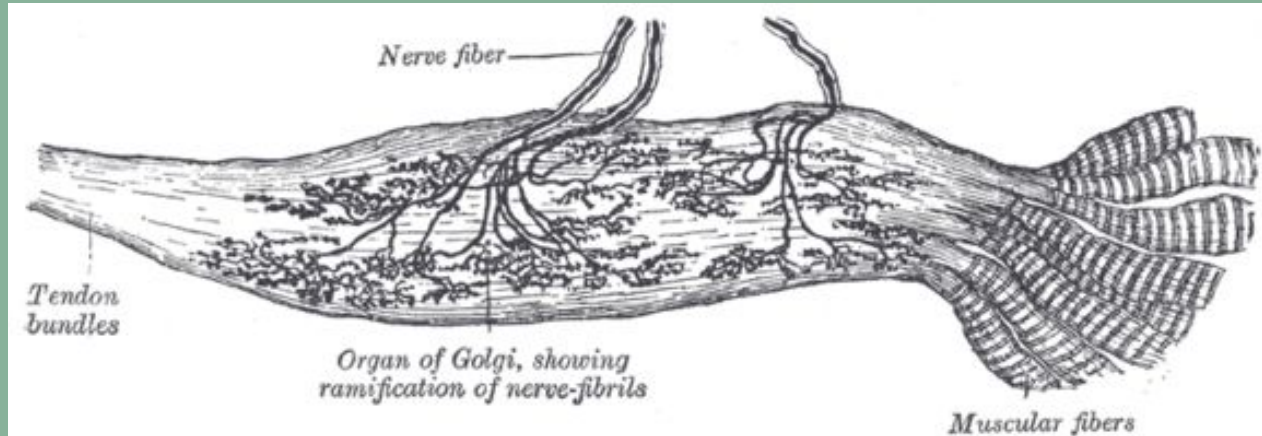
Introduction



The golgi tendon organ (GTO) functions to give the brain proprioception to its skeletal muscles



- Stress Sensitive Cation Channel



[1]



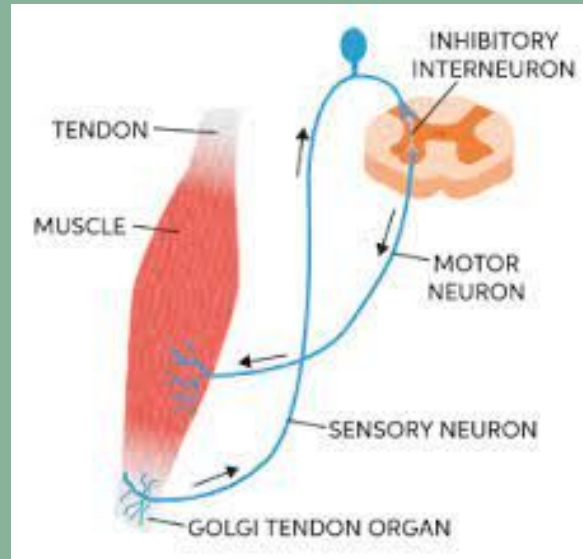


Introduction



There are key barriers to creating GTO on a chip

- Neurotendinous spindle structure



[2]



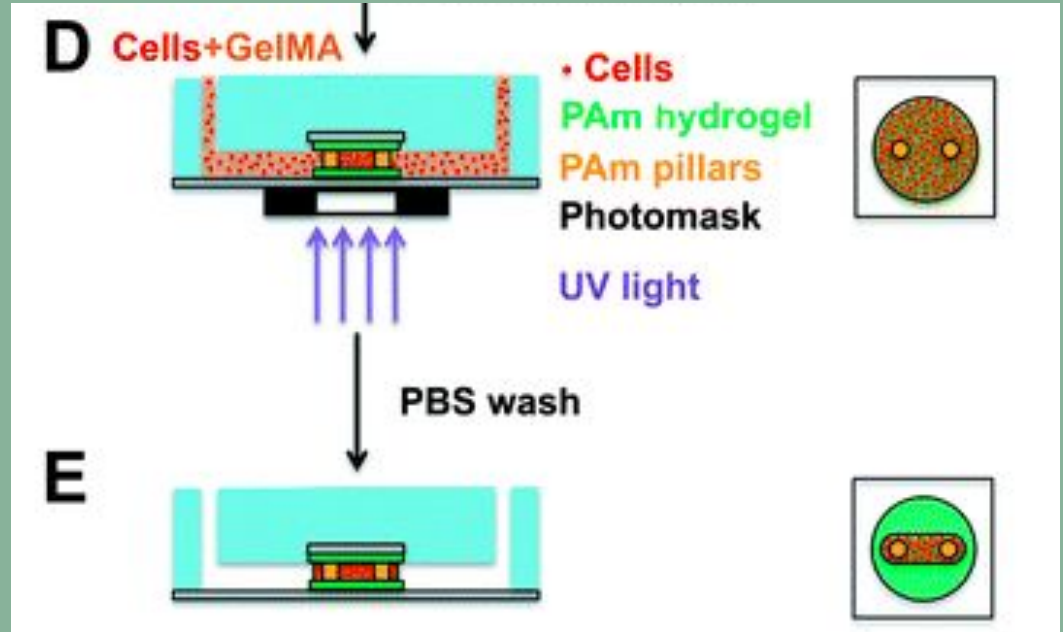


Introduction



Muscle on a chip models have been previously developed

- GTO behavior not isolated



[3]



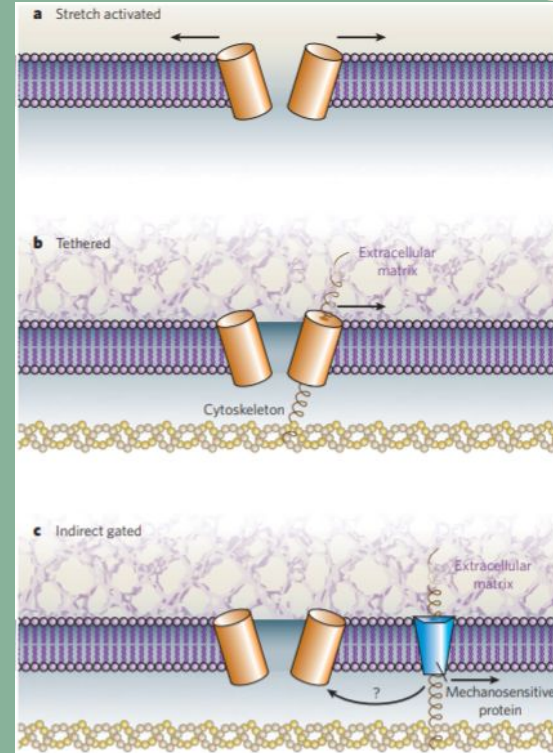


Introduction



Stress activated channels are applicable to approximations of other bodily systems:

- Inner ear
- Lungs
- Bladder



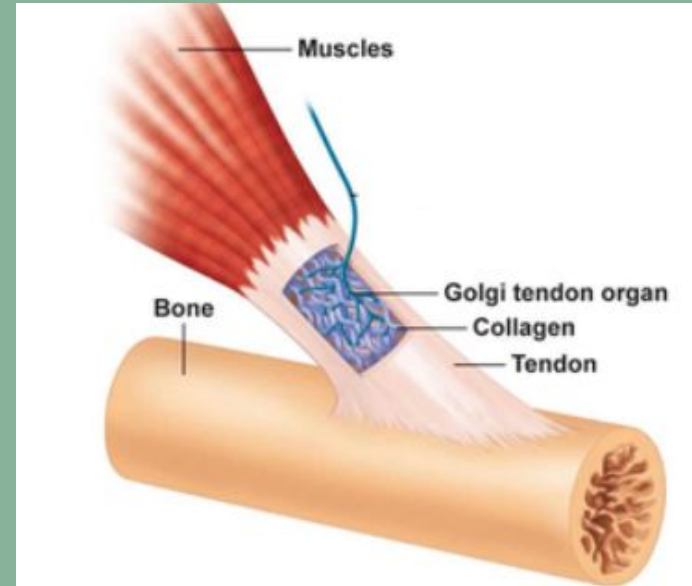


Introduction



There are diseases associated with muscle function that can be more easily studied with muscle on a chip models

- Cachexia
- Sarcopenia



[5]



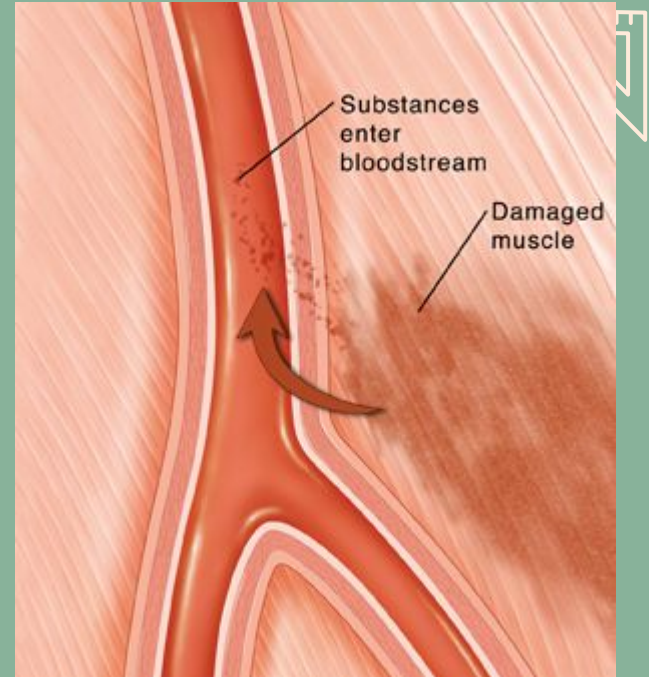


Introduction



Various drug side effects on muscle tissue could be more accurately studied with muscle on a chip systems that contained GTOs.

- Metformin (treats diabetes)
- Statin (treats high cholesterol)



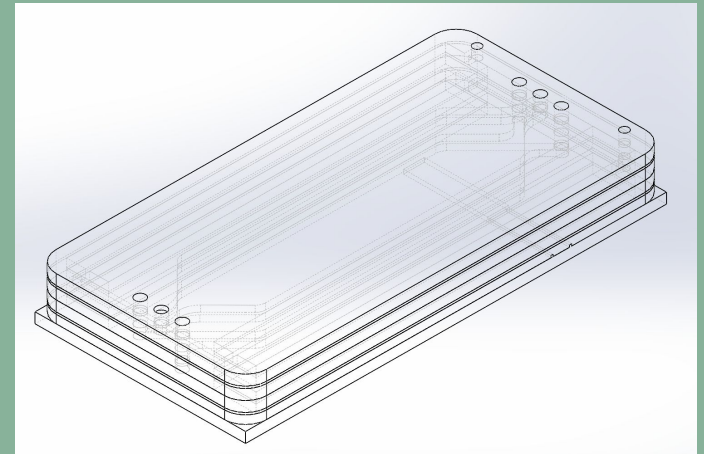
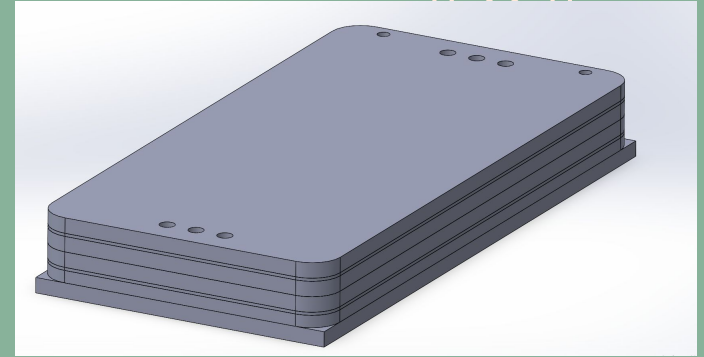
[6]





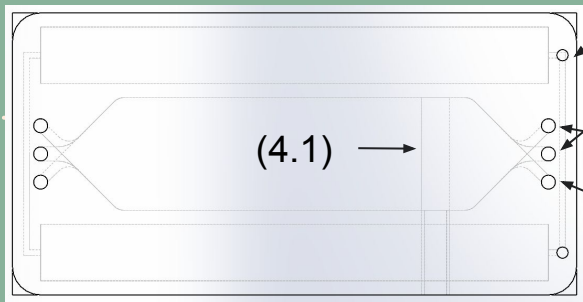
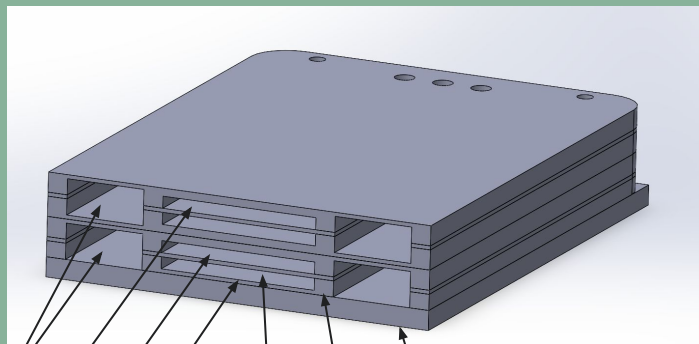
Device

- Simulate GTO operation
- Inspired by pulmonary and muscle specific BioMEMS devices
- All-in-one design
 - Cell culture
 - Cell stretching
 - Golgi tendon simulation
- Open or closed-loop feedback operation
 - Calibration
 - Comparison



Layout

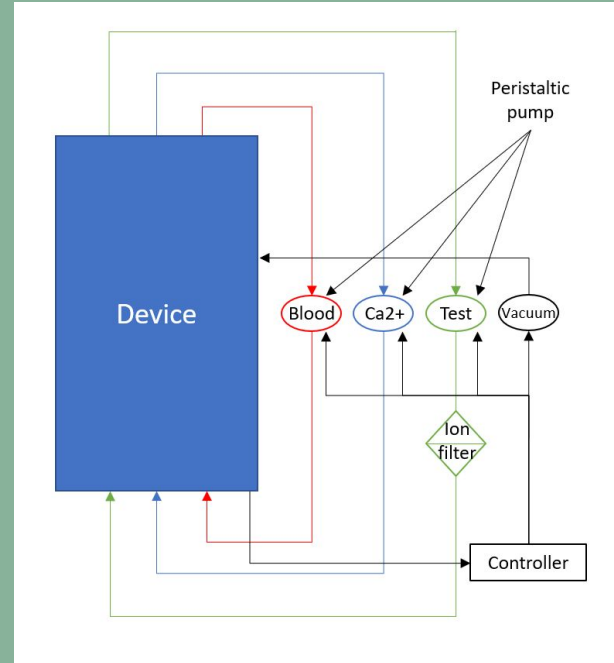
- Vacuum channels (1)
- Blood channels (2)
- Ionic solution channel (3)
- Test solution channel (4)
- Test solution channel (FET location) (4.1)



Polymer base
PDMS structural layer
PDMS membrane layer

System

- 1 Controller
- 3 Peristaltic pumps
- 2 Vacuum pumps
- 3 independent circuits
 - Oxygen rich blood
 - High concentration ion solution
 - Test solution (filtered)
- FET and Capacitive pressure sensor feedback

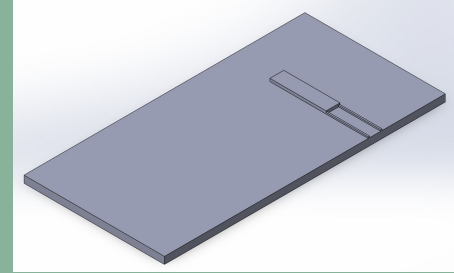




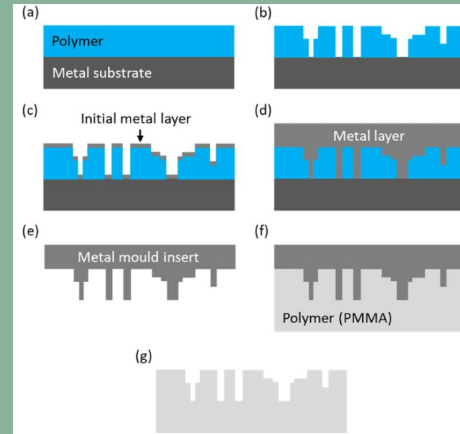
Base Plate Fabrication



- Silicon Surface Micromachining
 - Fully compatible with microfluidic sensors
 - Low Cost

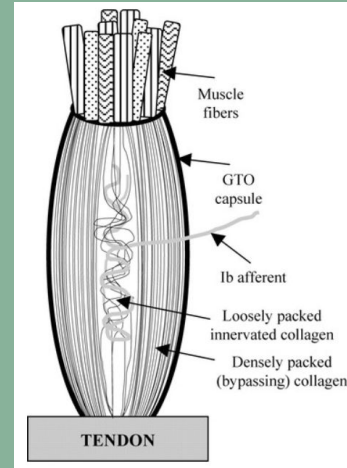


- LIGA
 - Constructs microstructures made of polymers, ceramics, metals, etc.
 - Easily integratable with biomimetic sensors
 - Force/pressure changes resistivity of conductive polymers
 - Can act as actuator between systems



* Membrane Fabrication

- Needs to behave similar to a GTO
- Stretching activated by two collagen sections
 - Innervated collagen near center of structure
 - Packed with GTO afferents
 - Stretches and aligns when activated
 - Dense collagen forming capsule surface
 - Don't interact with afferent
 - Packed tighter near ends of GTO
- Create similar collagen network without muscle fibers, tendon, of afferent



[8]

$$T^{col} = K^{col} \times A^{col} \times \text{sign}(x - x_{rest}) \times \left\{ \left[\frac{\text{abs}(x - x_{rest}) + x_{rest}}{x_{rest}} - 0.99 \right]^3 - 10^{-6} \right\}$$

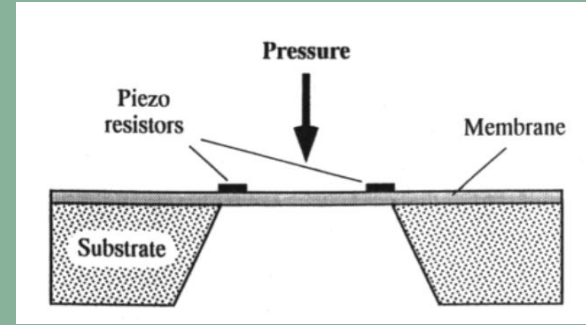
[8]



Biomimetic Membrane Sensors



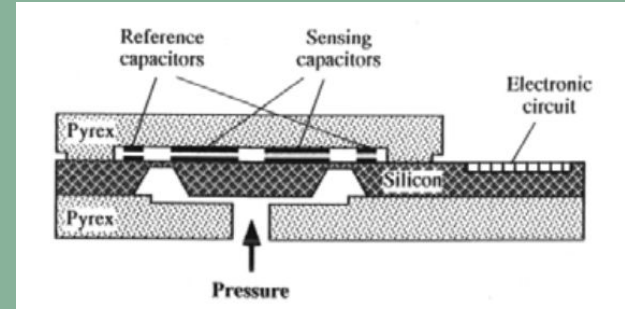
- Piezoelectric Pressure Sensor
 - Used on small, deflectable membranes
 - Deflection → Change in resistance



[9]



- Capacitive pressure sensor
 - Uses change in capacitance between two metal plates
 - Higher linearity, sensitivity, and stability
 - Higher production cost and less effective for complex signals



[9]



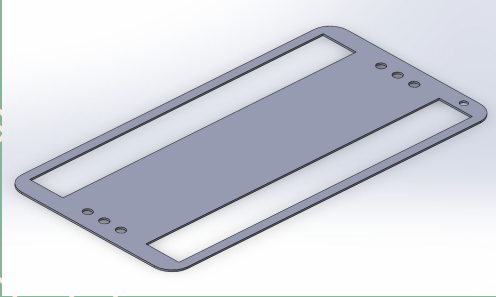
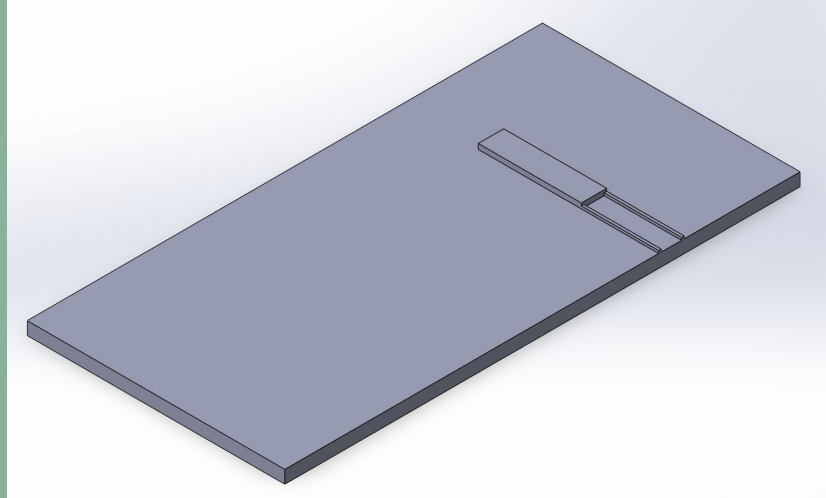
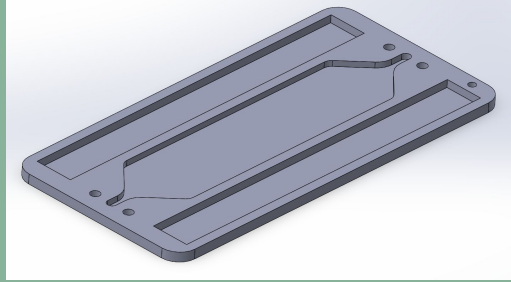


Ion Membrane Fabrication



- Pores open via vacuum stretching
 - Activated when capacitor displacement is detected
- PDMS layer
 - Highly flexible to deform with the vacuum
- Fluorine based Reactive Ion Etching
 - Complements molding with SU-8 photoresist







Biocompatibility



External device with no body contact:

- No ISO or FDA requirements

Material requirements:

- Membrane
 - Skeletal muscle growth
 - Channel geometry for ion transfer
- Channel structure
 - Limiting ion absorption and diffusion
- Effective ion filters for FET unsaturation



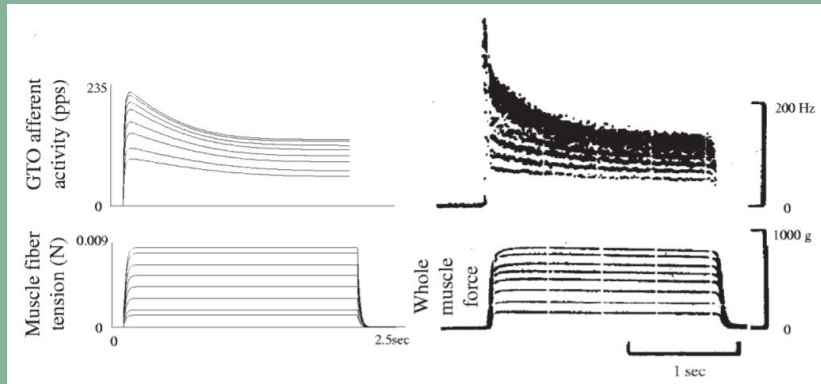


Testing (1)



Golgi Tendon Property

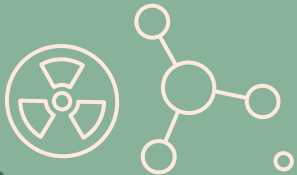
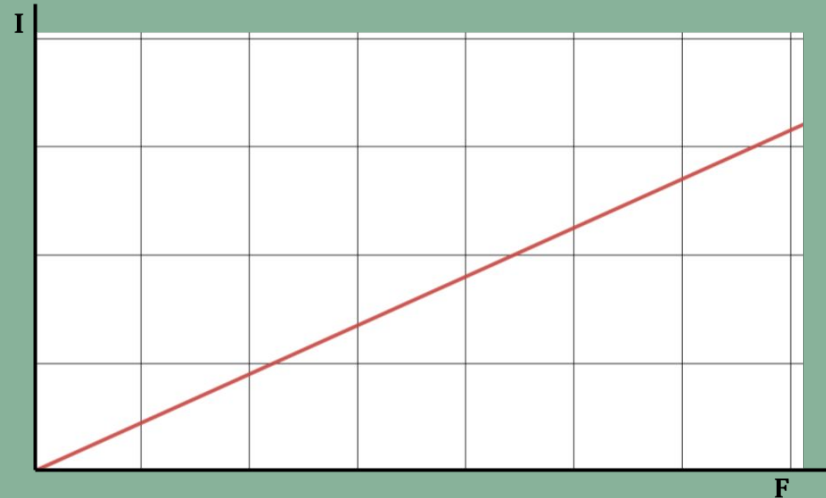
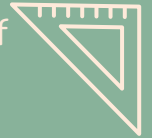
Tension Proportionality (Steady State GTO Activation is Linearly Proportional to Muscle Tension) [10]



[8]

Method for Testing

Apply constant voltage to FET, apply range of vacuum pressures in chambers. Graph FET current (as $t \rightarrow \infty$) against vacuum pressure:



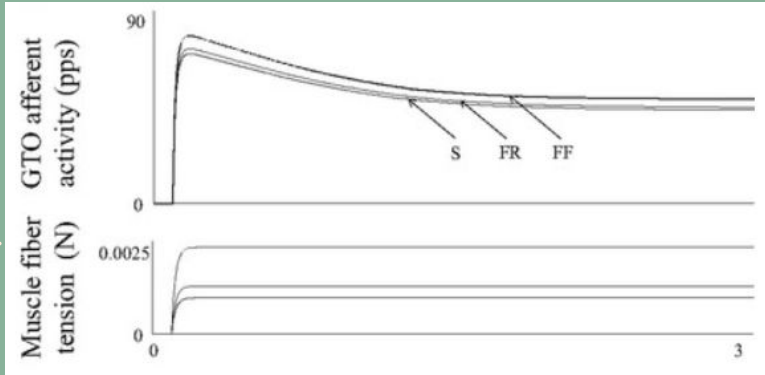


Testing (2)



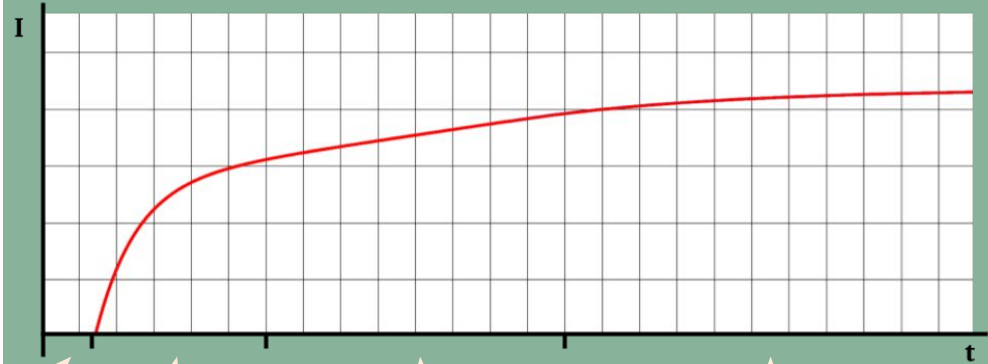
Golgi Tendon Property

Stress Relaxation (GTO Typically modeled as Standard Linear Viscoelastic Solid) [8]



Method for Testing

Apply constant strain in vacuum chambers, apply constant voltage to FET, verify FET current resembles:



Gate Threshold not met

Stress Relaxation Dominates

Passive Stress Dominates

Ligand Binding Dominates



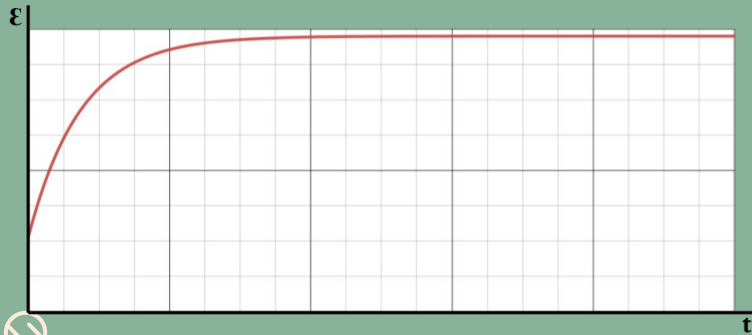


Testing (3)



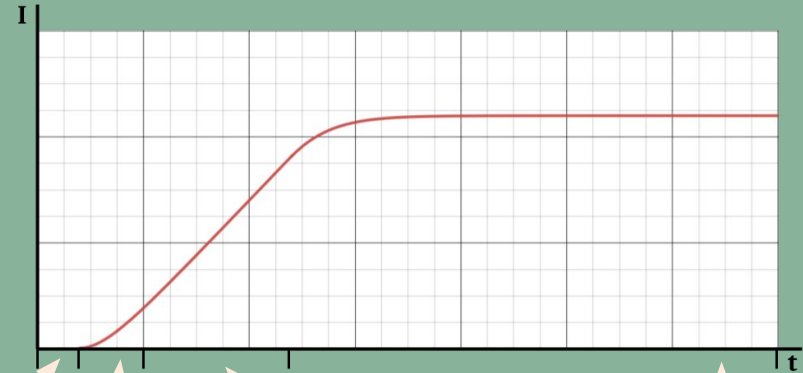
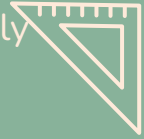
Golgi Tendon Property

Creep (GTO Typically modeled as Standard Linear Viscoelastic Solid) [1]



Method for Testing

Apply constant stress in vacuum chambers, apply constant voltage to FET, verify FET current resembles:



Gate Threshold
not met

Initial Stress
Dominates

Creep
Dominates

Ligand Binding
Dominates



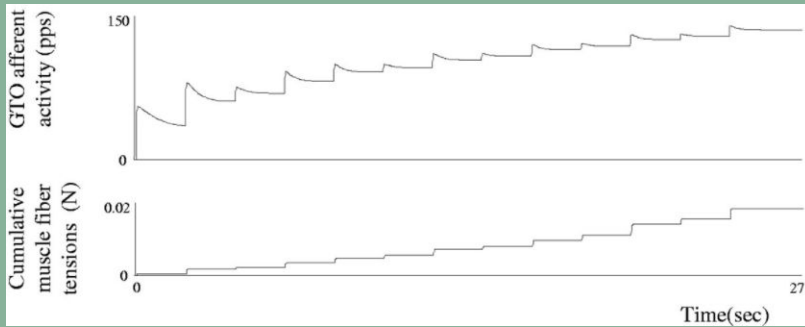


Testing (3)



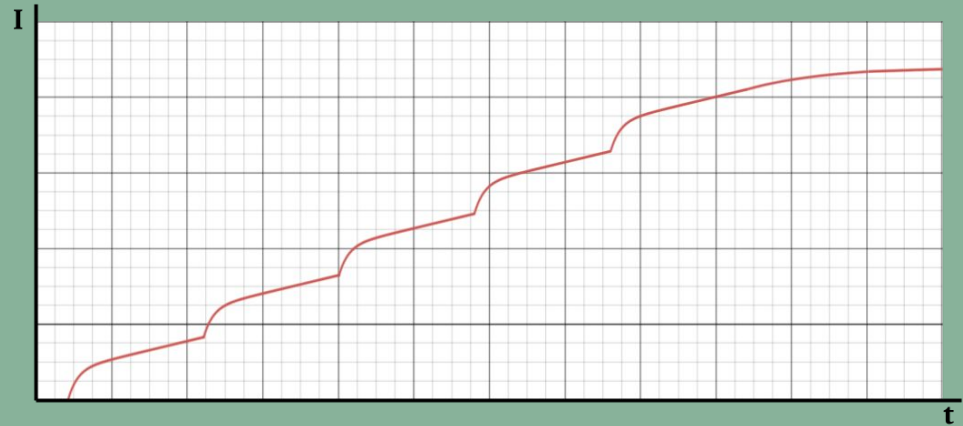
Golgi Tendon Property

Summation Response (GTO Activity increases as more motor units engaged) [8]



Method for Testing

Apply constant voltage to FET, apply vacuum pressure as series of step functions with diminishing amplitude increases. [8] Verify FET current resembles:





Testing (3)



Golgi Tendon Property

Ion Selectivity (Stretch Sensitive Ion Channels are only meant to release Ca^{2+})

Method for Testing

Repeat stress relaxation test with Na^{+} in ion chamber:





Testing (4)

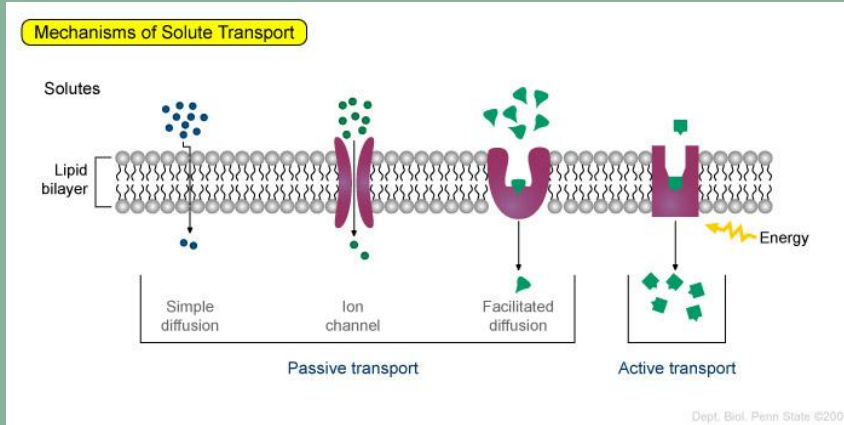


Golgi Tendon Property

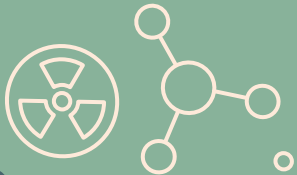
Extracellular Calcium concentration dissipates after Golgi Tendon activation ends

Method for Testing

Apply constant isFET voltage and pressure, wait until isFET current reaches steady state, then deactivate pressure chambers:



[11]





Testing (5)

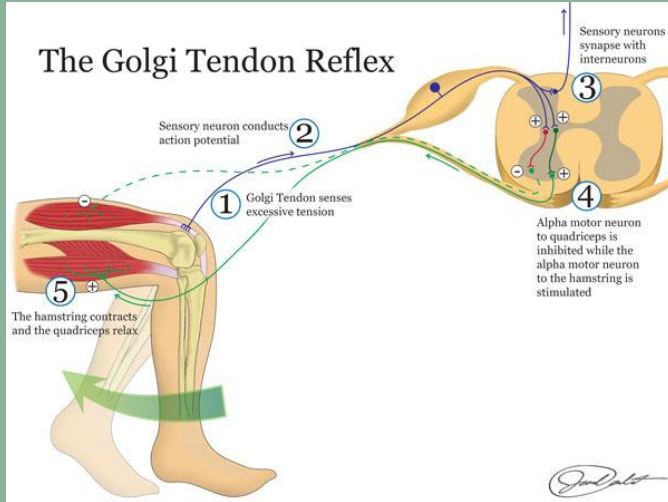
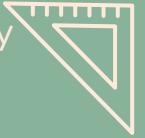


Golgi Tendon Property

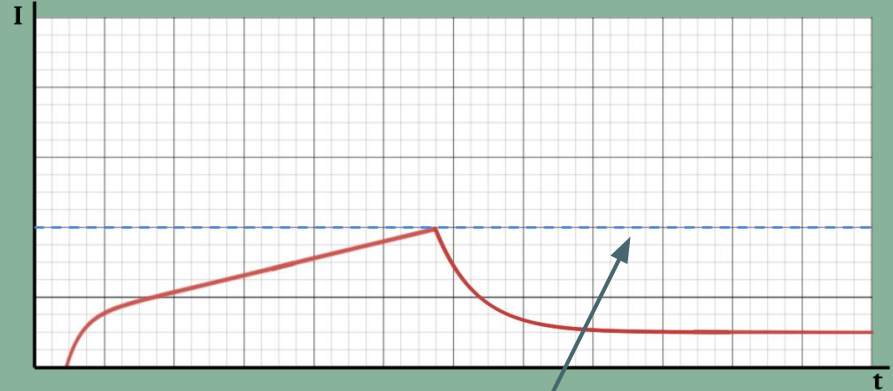
Reflex (GTO works to prevent harmful levels of muscle tension) [12]

Method for Testing

Apply linearly increasing vacuum pressure, verify GTO feedback downsteps vacuum at set value:



[13]



Force Threshold (Current Max Force Levels At)





Limitations



1. No proper modeling of action potential or nerve fibers
2. Only modeling one GTO fiber
3. In a true GTO, passive stretch doesn't cause activation
4. Standard linear elastic solid is an approximation of material properties

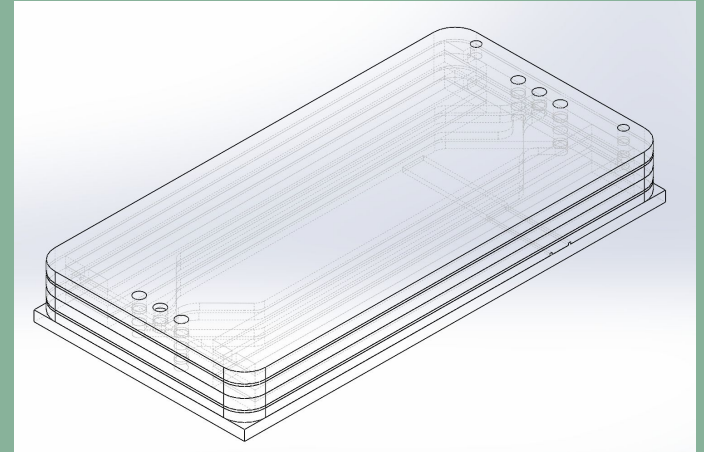




Conclusion



- GTO/Muscle on a chip not fully developed
- Device limited to full GTO scale, but models main ion activation behavior
- Future Directions
 - Device dimensioning
 - Test how GTO responds to different drugs
 - Model different disease state responses
 - Apply principles to model other mechanosensitive channels in the body
- Future Improvements/Revisions
 - Populate with true mechanosensitive channels
 - Integrate with nervous system on a chip





Sources



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- [12] Hall & Guyton (2006), Golgi Tendon Reflex, pp. 679–680
- [13] https://content.byui.edu/file/a236934c-3c60-4fe9-90aa-d343b3e3a640/1/module9/readings/somatic_reflexes.html
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